

Accepted Manuscript



Deep repetitive transcranial magnetic stimulation with H-coil on lower limb motor function after stroke: a pilot study

Raffaella Chieffo, MD Serena De Prezzo, MD Elise Houdayer, PhD Arturo Nuara, MD Giovanni Di Maggio, MD Elisabetta Coppi, MD Laura Ferrari, MD Laura Straffi, MD Francesca Spagnolo, MD Svetla Velikova, MD, PhD Maria Sessa, MD Mauro Comola, MD Abraham Zangen, PhD Giancarlo Comi, MD Letizia Leocani, MD, PhD

PII: S0003-9993(14)00179-8

DOI: [10.1016/j.apmr.2014.02.019](https://doi.org/10.1016/j.apmr.2014.02.019)

Reference: YAPMR 55758

To appear in: *ARCHIVES OF PHYSICAL MEDICINE AND REHABILITATION*

Received Date: 18 November 2013

Revised Date: 29 January 2014

Accepted Date: 18 February 2014

Please cite this article as: Chieffo R, De Prezzo S, Houdayer E, Nuara A, Di Maggio G, Coppi E, Ferrari L, Straffi L, Spagnolo F, Velikova S, Sessa M, Comola M, Zangen A, Comi G, Leocani L, Deep repetitive transcranial magnetic stimulation with H-coil on lower limb motor function after stroke: a pilot study, *ARCHIVES OF PHYSICAL MEDICINE AND REHABILITATION* (2014), doi: 10.1016/j.apmr.2014.02.019.

This is a PDF file of an unedited manuscript that has been accepted for publication. As a service to our customers we are providing this early version of the manuscript. The manuscript will undergo copyediting, typesetting, and review of the resulting proof before it is published in its final form. Please note that during the production process errors may be discovered which could affect the content, and all legal disclaimers that apply to the journal pertain.

Running head: Lower limb H-coil rTMS in chronic stroke**Title: Deep repetitive transcranial magnetic stimulation with H-coil on lower limb motor function in chronic stroke: a pilot study**

Raffaella Chieffo, MD¹; Serena De Prezzo, MD¹; Elise Houdayer, PhD¹; Arturo Nuara, MD¹; Giovanni Di Maggio, MD¹; Elisabetta Coppi, MD¹; Laura Ferrari, MD¹; Laura Straffi, MD¹; Francesca Spagnolo, MD¹; Svetla Velikova, MD, PhD¹; Maria Sessa, MD¹; Mauro Comola, MD¹; Abraham Zangen, PhD²; Giancarlo Comi, MD¹; Letizia Leocani, MD, PhD¹.

¹Scientific Institute Vita-Salute University San Raffaele; Neurological Dep.t; Experimental Neurophysiology Unit, INSPE – Institute of Experimental Neurology; Milan, Italy

²Department of Life Sciences Ben-Gurion University, Beer-Sheva, Israel

Corresponding Authors: Letizia Leocani, MD, PhD, and Raffaella Chieffo, MD, Institute of Experimental Neurology, Dep.t of Neurology, Scientific Institute and University Hospital San Raffaele, Milan. Via Olgettina 60, 20132 Milan, Italy. Tel: ++39 02 26433092. Fax: ++39 02 26433085; email: letizia.leocani@hsr.it

Conflicts of interest

A. Zangen is a key inventor of deep TMS H-coils and has financial interest in Brainsway Ltd. The other authors declare no conflicts of interest related to the present study.

Acknowledgments

Supported through the Joint Italian-Israeli laboratory on Brain modulation in neuroimmune, neurodegenerative, and mental disorders (Italian Ministry of Foreign Affairs). Dr R. Chieffo and dr F. Spagnolo participated in this study as partial fulfillment of her PhD in Molecular Medicine, Program in Experimental Neurology, San Raffaele University, Milan, Italy.

1 **Deep repetitive transcranial magnetic stimulation with H-coil on lower limb motor**
2 **function after stroke: a pilot study**

3 **Abstract**

4 **Objectives:** To assess the efficacy of high frequency (20 Hz) brain stimulation on lower limb
5 motor function in subjects with chronic (> 6 months) subcortical stroke in a double-blind,
6 placebo-controlled crossover study.

7 **Design:** double-blind, placebo controlled, crossover study

8 **Setting:** University hospital.

9 **Participants:** ten right-handed subjects affected by a first-ever subcortical stroke in the
10 territory of the middle cerebral artery were included in this study.

11 **Interventions:** rTMS was delivered with the H-coil, specifically designed to target deeper
12 and larger brains regions. Each subject received both real and sham rTMS in a random
13 sequence. The two rTMS cycles (real or sham) were composed of 11 sessions each,
14 administered over 3 weeks and separated by a 4-week wash-out period.

15 **Main Outcome Measures:** lower limb functions were assessed by the lower limb Fugl-
16 Meyer (FM) scale, the 10 meters walking test (10MT) and the six minutes walking test
17 (6MWT), before and 1 day after the end of each treatment period, as well as at a 4-week
18 follow-up.

19 **Results:** real rTMS treatment was associated with a significant improvement in lower limb.
20 This effect persisted over time (follow-up) and was significantly greater than that observed
21 with sham stimulation. A significant increase in walking speed was also found after real
22 rTMS but this effect did not reach statistical significance in comparison with the sham
23 stimulation.

24 **Conclusions:** these data demonstrated that 3 weeks of high-frequency deep rTMS could
25 induce long-term improvements in lower limb functions in the chronic post-stroke period,
26 lasting at least 1 month after the end of the treatment.

27

28 **Keywords:** stroke, lower limbs, rehabilitation, rTMS, H-coil.

29

30 **List of abbreviations**

31 rTMS: repetitive transcranial magnetic stimulation; FM: Fugl-Meyer scale; 10MT: 10
32 meters walk test; 6MWT: 6 minutes walk test.

33

34 Stroke is a leading cause of long term disability and non invasive brain stimulation
35 techniques have been recognized as a promising intervention for the treatment of post-stroke
36 motor deficits¹⁻³. Although the ability to walk is impaired in more than 80% of post-stroke
37 subjects⁴, the pathophysiological reorganization of lower limb motor areas after stroke is still
38 unclear as relatively fewer data are available compared with the upper extremity. A study
39 performed with Near-infrared Spectroscopic Imaging System in stroke subjects during
40 walking showed that, similarly to upper limb, the cortical activation patterns of motor,
41 premotor and supplementary lower limb motor cortex was greater for the unaffected
42 hemisphere rather than for the affected hemisphere⁵. The latter data suggest that the concept
43 of interhemispheric competition, proposed for homologous upper limb motor areas⁶, might
44 be applied even in the case of lower extremity post-stroke recovery. Consistently,
45 improvements of gait parameters of the paretic lower limb have been found associated with a
46 reduction of the interhemispheric asymmetry of the primary sensori-motor cortical activations

47 ⁷. Wang and colleagues ⁸ first evaluated in a placebo controlled study, the therapeutic effect
48 of task-oriented training associated with 1Hz repetitive transcranial magnetic stimulation
49 (rTMS) (with the figure-of-eight coil) performed to inhibit the unaffected lower limb motor
50 cortex in chronic stroke subjects. The authors found that inhibitory rTMS enhanced the effect
51 of task-oriented training on walking performance and motor control ability, leading to a more
52 symmetric gait pattern. Recovery of motor deficits was associated with a reduction of the
53 interhemispheric asymmetry of the leg motor excitability.

54 However, in the chronic phase after stroke, the interhemispheric competition, at least
55 in the upper limb, has been found less pronounced than in the subacute period, and it is
56 commonly observed that the transcallosal asymmetry slows down with time ⁹. Moreover, as
57 bi-hemispheric control of foot movements in healthy subjects have been proposed ¹⁰ one
58 could hypothesize a positive, rather than detrimental role of the unaffected lower extremity
59 motor system in recovery mechanisms occurring after stroke. Moreover, in a more recent
60 placebo controlled cross-over study, a single session of high-frequency rTMS, over the leg
61 motor area bilaterally using a double-cone coil, has been reported to significantly improve
62 walking performance for 20 minutes after stimulation in comparison with sham stimulation in
63 a group of chronic post-stroke subjects ¹¹.

64 The purpose of our study was to assess the safety and efficacy of bilateral excitatory,
65 high frequency rTMS over the lower limb cortical motor representation in chronic subcortical
66 stroke. To reach the lower limb cortical motor areas, deeply located in the mesial cortical
67 surface of the hemispheres, we delivered rTMS was delivered using the H-coil, designed to
68 effectively stimulate at about a depth of 3-5 cm below the skull ^{12, 13}. Compared with the
69 standard figure-of-eight coil, the H-coil has been reported to require lower intensities to
70 obtain lower limb motor responses¹⁴ and larger volumes of the induced electric field ¹⁴,
71 ¹⁵. The H-coil rTMS has been reported effective in the treatment of psychiatric disorders such

72 as major depressive disorder or bipolar depression^{13, 16, 17}. Recently, analgesic effects in
73 subjects with painful diabetic neuropathy were obtained using deep rTMS with H-coil
74 targeting the leg motor cortex¹⁵.

75 We hypothesized that high-frequency rTMS delivered with the same H-coil type over
76 the lower limb motor cortical areas could improve the paretic lower limb function in chronic
77 post-stroke subjects.

78

79 **Methods**

80 **Subjects**

81 Ten right-handed subjects affected by a first-ever stroke in the territory of the middle
82 cerebral artery were included in this study. The inclusion criteria for participants were:
83 evidence of acute brain lesion on computerized tomography-CT or magnetic resonance-MR
84 scans at symptoms onset; time between the stroke event and the enrolment in the protocol
85 ranging from 6 months to 3 years (chronic phase); age at admission between 25 and 80 years;
86 ability to walk independently for at least 10 meters, even with assistive devices (cane, ankle-
87 foot orthoses etc.). Exclusion criteria were: history of other neurological disorders, lesions
88 involving the cortical lower limb motor representation, use of drugs acting on central nervous
89 system; presence of contraindications to undergo rTMS such as pregnancy, cochlear
90 implants, neurostimulator, metal in the brain or skull, cardiac pacemaker, history of epilepsy
91 or head trauma diagnosed as a concussion¹⁸.

92 Subjects' age at admission ranged between 49 and 74 years (mean 62.2 years). All
93 subjects suffered from sub-cortical stroke, the affected hemisphere was the right in 6 subjects,
94 while the other 4 subjects had a lesion in the left hemisphere. Subjects' data and lesion
95 localization are reported in Table 1.

96 All subjects gave their signed written informed consent to participate in the study that was
97 approved by our local ethics committee (DO/MS/ER protocol number: 111/11).

98 **Procedures**

99 We performed a double blind, placebo controlled crossover study. Each subject
100 received both real and sham rTMS treatment cycles separated by a four week washout period
101 in a random sequence (sham-real or real-sham). After full randomization, performed through
102 administrative personnel not involved in the protocol, each participant was assigned two
103 blank-coded magnetic cards (A and B), to be used respectively in the first and second cycle.
104 Each card pair contained opposite types of treatments (sham and real). Consecutive subjects
105 were randomized with a global 1:1 ratio, so that 5 participants performed the real-sham and 5
106 the sham-real treatment sequence. Active or sham modes were determined by a switch
107 controlled through the assigned magnetic card. This procedure ensured blindness of subjects,
108 examiners and treating personnel. Each treatment cycle lasted 3 weeks for a total of 11 high-
109 frequency rTMS sessions (5 in the first week and 3 in the second and third weeks) (Figure 1).
110 No specific motor task involving the lower limb was associated to the rTMS treatment.

111 **Deep rTMS**

112 A Magstim Rapid² stimulator (Magstim Company Ltd, Whitland, Dyfed, UK) was
113 coupled with an H-coil (Brainsway Ltd, Jerusalem, Israel) to deliver rTMS. The H-coil,
114 designed for effective activation of hand or leg motor cortex, contained 14 windings. Three
115 medial groups conduct current along a postero-anterior axis, and two other groups return
116 currents in the opposite (anterior-posterior) direction ¹⁵. Resting motor threshold was
117 measured after positioning the H-coil over the vertex on the optimal location for obtaining
118 lower limb motor responses. Resting motor threshold was defined as the minimal intensity
119 evoking visible movements on either lower limb or electromyographic motor evoked

120 potentials on tibialis anterior muscle that were monitored bilaterally, with amplitude of 50 µV
121 or higher in 5 out of 10 stimuli, using 1% increments of stimulator output. Then, the H-coil
122 was tightly fixed on the same position with a belt and the sham or real rTMS treatments were
123 delivered (90% of resting motor threshold or up to 84% maximal stimulation output; 30 trains
124 at 20 Hz, 60 sec inter-train interval; total number of pulses 1500). Sham stimulation was
125 performed by activating a sham coil placed in the same stimulation helmet designed to mimic
126 a similar acoustic artifact and some scalp sensation but without inducing an effective field
127 inside the brain. The sham stimulation is, indeed, non tangentially orientated on the scalp,
128 with components cancelling the electric field, which is rapidly reduced as a function of
129 distance¹². Each rTMS session lasted about 30 minutes.

130 **Safety**

131 Vital signs were recorded before and after each rTMS session. Participants were asked
132 to report every possible adverse event; especially the most frequently reported side effects
133 such as headache, or dizziness. We also performed continuous visual monitoring of
134 participants throughout all treatment sessions, excluding the occurrence of involuntary
135 movements suggesting stimulation above motor threshold or seizures.

136 **Clinical evaluation**

137 Clinical evaluation was performed before and one day after the end of the treatment
138 period, as well as at a four-week follow-up (which served as baseline for the second treatment
139 cycle) (Figure 1). The residual neurological deficit (National Institutes of Health Stroke
140 Scale-NIHSS) and the degree of disability (Barthel Index and modified Rankin Scale) were
141 quantified at enrollment.

142 The primary outcome was the Fugl-Meyer (FM) assessed for the affected lower limb. The
143 motor score ranges from 0 (hemiplegia) to a maximum of 34 points (normal motor
144 performance). It includes items measuring synergic and simple movements, coordination, and
145 reflex at the hip, knee, and ankle levels ¹⁹. As exploratory measures (secondary outcome) we
146 used:

147 - 10 meter walk test (10MT): the subject was asked to walk as quickly as possible, back
148 and forth, along a 10-meter path marked by a starting and arriving line on the floor.

149 Assistive devices were allowed except the walker. The task was administered twice in
150 a row. The best time of the two trials was considered for our data analysis.

151 - 6 minute walk test (6MWT) (secondary outcome): this test measured the distance
152 walked in a period of 6 minutes ²⁰.

153

154 **Statistical analysis**

155 Given the exploratory nature of this pilot trial, no sample size determination was
156 performed. Statistical analysis was performed using the SPSS software (version 13.0, SPSS
157 Inc., USA). After verifying the normal distribution with the Kolmogorov-Smirnov Test,
158 parametric tests were used. When appropriate, the Geisser-Greenhouse procedure was applied
159 to correct degrees of freedom. The significance level was set at $p \leq 0.05$ for all analyses.

160 Changes over time in clinical outcomes after real or sham (9 subjects) treatment were
161 first evaluated. Absolute clinical measures (lower limb FM, 10MT and 6MWT) underwent
162 two separate one-way ANOVA for repeated measures for the real and the sham group
163 respectively, with Time as within subject factor (baseline, end of treatment and follow-up).

164 To directly compare the effects of real and sham treatment on clinical outcomes we
165 calculated the percent change to the relative baseline of clinical scores obtained immediately
166 after sham or real treatment (end of treatment) and after 1-month follow-up as follows:

167 $\% \text{ end of treatment} = [(\text{end of treatment} - \text{baseline}) / \text{baseline}] \times 100;$

168 $\% \text{ follow-up} = [(\text{follow-up} - \text{baseline}) / \text{baseline}] \times 100$

169 Then, a two-way ANOVA for repeated measures was performed using “treatment”
170 (real and sham) and “time” (end of treatment and follow-up) as within subject factors. If a
171 significant main effect was found, post-hoc comparisons were performed using paired
172 Student’s T-tests. Differences in the two baseline measurements (before real and sham
173 treatment) were evaluated with paired T-tests.

174 **Results**

175 Of the 10 participants, results will be presented for 9 since one left the study because
176 of a cardiac disease and was therefore not included in the statistical analysis (patient 6-Table
177 1). Lower limb motor responses, at rest or with facilitation through voluntary contraction,
178 were obtained in all subjects.

179 **Safety**

180 No subject reported any adverse effects related to rTMS, including seizures. No
181 significant changes in blood pressure levels were observed throughout the protocol periods.
182 Finally, the applied stimulation parameters were well tolerated by all subjects.

183 **Clinical outcomes**

184 The two treatment baselines (T_1 vs T_3 ; n=9, paired T-test) of the clinical measures were
185 not significantly different (lower limb FM p=0.1; 10MT p=0.5; 6MWT p=0.4).

186 No absolute significant changes over time in any clinical measure were found after
187 sham treatment (repeated measures ANOVA: lower limb FM: F=0.8, p=0.4; 10MT F=0.7,
188 p=0.4; 6MWT F=0.7, p=0.4). A significant effect of “time” factor on lower limb FM and

189 10MT ($F=17.1$, $p<0.001$ and $F=3.7$, $p=0.05$ respectively) but not on 6MWT ($F=0.2$, $p=0.1$)
190 was found in the real group. The post-hoc analysis revealed a significant improvement of
191 lower limb FM score between baseline and both end of treatment evaluations (baseline *vs* end
192 of treatment: $p=0.009$; baseline *vs* follow-up $p=0.001$) as well as a persisting improvement in
193 the follow-up period (end of treatment *vs* follow-up $p=0.05$). The improvement at follow-up
194 *vs* baseline suggests a carry-over effect up to the second baseline measurements for the real
195 treatment (Figure 2). We also found a significant amelioration in 10MT performance at the
196 end of the real treatment in comparison with baseline (baseline *vs* end of treatment $p=0.04$).
197 The persistent improvement after 1 month follow-up did not reach significance (baseline *vs*
198 follow-up $p=0.07$) (Table 2).

199 Comparing the effects of real and sham stimulation, the ANOVA analysis showed a
200 significant effect of “treatment” factor ($F=12$, $p=0.008$) as well as a significant interaction
201 between “time” and “treatment” factors ($F=11.3$, $p=0.01$) only on lower limb FM score
202 (6MWT and 10MT: n.s.). The percentage improvement of lower limb FM resulted
203 significantly greater for real *vs* sham stimulation at the end of treatment and even more at 1-
204 month follow-up ($p=0.01$ and $p=0.006$ respectively). Moreover, clinical gains with real
205 stimulation significantly progressed between end of treatment and follow-up evaluations (end
206 of treatment *vs* follow-up: $p=0.04$) (Figure 3).

207

208 **Discussion**

209 The deep representation of lower limb muscles in the human brain makes it difficult to
210 approach with standard non-invasive stimulation techniques. So far, few studies have been
211 published about potential therapeutic rTMS application on post-stroke walking deficits. A
212 recent open study showed that a protocol consisting in 20 sessions of high-frequency rTMS
213 delivered with double cone coil associated with mobility training is safe and can improve

walking function after stroke²¹. To our knowledge, this is the first placebo controlled study evaluating the safety and the therapeutic effect of deep non invasive brain stimulation delivered with H-coil over the lower limb motor cortex bilaterally in post-stroke gait disturbance. For this pilot study we enrolled participants with stroke in the territory of the middle cerebral artery and excluded those with stroke in the territory of the anterior cerebral artery, in order to avoid cortical lesions of the target lower limb representation, mainly for safety reasons (i.e. to avoid epileptic activation). Moreover, subjects with lesions involving the motor cortex have been reported as less likely to benefit from rTMS treatment²². Our results suggest an effective role of deep high-frequency rTMS in ameliorating lower limb motor function, especially regarding the Fugl-Meyer lower limb scores. Evaluating the duration of such effect over time, participants not only maintained the benefits of the H-coil treatment at one month follow-up, but they continued to ameliorate after the end of the treatment, showing better scores at the follow-up compared to the post-rTMS evaluation. This could be explained by the long-lasting modulatory effects of non-invasive brain stimulation techniques^{23, 24}, probably potentiated by the daily use of the paretic lower limb. Consistently with this finding, the differences between real and placebo effects were mainly seen at the 4-week follow up. Although our data might be limited by a relatively short wash-out period, the crossover design of our study helped to point out the presence of a considerable long lasting effect of deep rTMS (Figure 2). Sham stimulation showed a weak effect on Fugl-Meyer lower limb score scale immediately after the end of treatment that faded away with time. Participants improved by 10.6 % on average after real rTMSvs 0.6 % after sham stimulation. An amelioration of about 30% of FM lower limb score in the experimental group has been obtained following 1 Hz rTMS over the unaffected lower limb motor area [23]. However, it is important to note that in the latter study rTMS was combined with task-oriented training, which is, by itself, beneficial for motor recovery²⁵. Indeed, an improvement of about 20% in

239 lower limb FM scale was found in the control group undergoing motor training associated
240 with sham rTMS. In our study, walking speed evaluated by the 10MT test significantly
241 increased only after real and not sham rTMS, but this effect did not reach statistical
242 significance in comparison with sham stimulation. Improvement after sham treatment on
243 10MT measurement was indeed greater than on FM lower limb scales, suggesting that pure
244 motor ability of the paretic limb, compared with walking speed, is less likely to improve after
245 sham stimulation. On the other hand, walking speed does not necessarily take into account
246 the quality of movement itself. Indeed, the 10MT test cannot allow to discriminate between
247 movement speed of the paretic and unaffected limbs. Moreover, all subjects included were all
248 autonomous in walking and therefore they might have had a limited margin for improvement.

249 The application of inhibitory rTMS over the contra-lesional motor cortex is based on
250 the model of interhemispheric competition after stroke established for the upper limb
251 extremity⁶. In fact, early hyperexcitability and increased interhemispheric inhibition of the
252 contralesional motor cortex have been demonstrated to the upper limb using TMS after
253 unilateral stroke^{26, 27}. However, in the post-stroke chronic phase the interhemispheric
254 competition is less pronounced than in the sub-acute period, as it is commonly observed that
255 the transcallosal asymmetry decreases with time⁹. Moreover, contralesional premotor and
256 motor cortex interference by TMS after chronic unilateral stroke worsens motor performance
257 during complex movement of the paretic hand. This finding has been interpreted as
258 suggesting a beneficial role of contra-lesional motor areas in effectively recovered complex
259 motor behavior after subcortical stroke²⁸. However, the mutual inhibition between
260 homologous motor areas can be modulated under physiological conditions. For example,
261 during movement preparation of the non-dominant hand the dominant hemisphere is
262 facilitated^{29, 30}. Moreover, studies on normal subjects suggest a bi-hemispheric control of
263 foot movements in healthy subjects. In particular, a more lateralized pattern of activation at

264 functional MRI has been found to finger movements versus lower limb joints, with increased
265 lateralization from proximal to distal lower joints³¹ implicating a different functional
266 specialization. Moreover, after training of the right lower limb an increased strength of the
267 homologous, with increased excitability of the corresponding motor cortex, has been reported
268 [30]. The latter findings implicate changes in functional interhemispheric connections
269 between the two motor cortices³². These findings could have important clinical implications
270 for subjects with reduced limb mobility after a stroke. Accordingly, our data suggest that
271 bilateral high frequency rTMS over the lower limb motor cortical representation may have a
272 beneficial role in motor recovery of the paretic limb. Further studies are needed to better
273 understand the mechanisms underlying this effect, in particular the role of plastic changes
274 over the motor cortex controlling the two lower limbs.

275

276 **Study limitations**

277 The small sample size is the major limitation of this study. Another limitation is the
278 crossover design of the study with a relatively short washout period with a carry-over effect
279 up to the second baseline measurements for the real treatment. Some feelings (e.g. scalp
280 sensations) may have differed in the placebo and real conditions. Therefore, the future use of
281 a questionnaire for study participants and evaluating physicians would be recommended to
282 help verifying that blinding is maintained throughout the conduction of the study.

283 **Conclusions**

284 Despite the limits of our study your main results suggests a potential beneficial role of
285 high-frequency rTMS delivered with the H-coil in improving lower limb motor function.
286 These findings represent the first evidence about a relevant but greatly unexplored field of
287 therapeutic application of non invasive neuromodulation.

288

289 **Suppliers**

- 290 a. Magstim Rapid² stimulator (Magstim Company Ltd, Whitland, Dyfed, UK)
291 b. H-coil (Brainsway Ltd, Jerusalem, Israel)

292

293 **References**

- 294 1. Hummel FC, Cohen LG. Non-invasive brain stimulation: a new strategy to improve
295 neurorehabilitation after stroke? Lancet Neurol 2006;5(8):708-12.
- 296 2. Alonso-Alonso M, Fregni F, Pascual-Leone A. Brain stimulation in poststroke
297 rehabilitation. Cerebrovasc Dis 2007;24 Suppl 1:157-66.
- 298 3. Bolognini N, Pascual-Leone A, Fregni F. Using non-invasive brain stimulation to
299 augment motor training-induced plasticity. J Neuroeng Rehabil 2009;6:8.
- 300 4. Duncan PW, Goldstein LB, Horner RD, Landsman PB, Samsa GP, Matchar DB.
301 Similar motor recovery of upper and lower extremities after stroke. Stroke 1994;25(6):1181-
302 8.
- 303 5. Miyai I, Yagura H, Oda I, Konishi I, Eda H, Suzuki T et al. Premotor cortex is
304 involved in restoration of gait in stroke. Annals of neurology 2002;52(2):188-94.
- 305 6. Nowak DA, Grefkes C, Ameli M, Fink GR. Interhemispheric competition after stroke:
306 brain stimulation to enhance recovery of function of the affected hand. Neurorehabil Neural
307 Repair 2009;23(7):641-56.
- 308 7. Miyai I, Yagura H, Hatakenaka M, Oda I, Konishi I, Kubota K. Longitudinal optical
309 imaging study for locomotor recovery after stroke. Stroke 2003;34(12):2866-70.
- 310 8. Wang RY, Tseng HY, Liao KK, Wang CJ, Lai KL, Yang YR. rTMS combined with
311 task-oriented training to improve symmetry of interhemispheric corticomotor excitability and

- 312 gait performance after stroke: a randomized trial. Neurorehabil Neural Repair
313 2012;26(3):222-30.
- 314 9. Swayne OB, Rothwell JC, Ward NS, Greenwood RJ. Stages of motor output
315 reorganization after hemispheric stroke suggested by longitudinal studies of cortical
316 physiology. Cereb Cortex 2008;18(8):1909-22.
- 317 10. Aglioti S, Dall'Agnola R, Girelli M, Marzi CA. Bilateral hemispheric control of foot
318 distal movements: evidence from normal subjects. Cortex 1991;27(4):571-81.
- 319 11. Kakuda W, Abo M, Nakayama Y, Kiyama A, Yoshida H. High-frequency rTMS
320 using a double cone coil for gait disturbance. Acta neurologica Scandinavica
321 2013;128(2):100-6.
- 322 12. Roth Y, Zangen A, Hallett M. A coil design for transcranial magnetic stimulation of
323 deep brain regions. J Clin Neurophysiol 2002;19(4):361-70.
- 324 13. Zangen A, Roth Y, Voller B, Hallett M. Transcranial magnetic stimulation of deep
325 brain regions: evidence for efficacy of the H-coil. Clinical neurophysiology 2005;116(4):775-
326 9.
- 327 14. Roth Y, Pell GS, Chistyakov AV, Sinai A, Zangen A, Zaaroor M. Motor cortex
328 activation by H-coil and figure-8 coil at different depths. Combined motor threshold and
329 electric field distribution study. Clinical neurophysiology 2014;125(2):336-43.
- 330 15. Onesti E, Gabriele M, Cambieri C, Ceccanti M, Raccah R, Di Stefano G et al. H-coil
331 repetitive transcranial magnetic stimulation for pain relief in patients with diabetic
332 neuropathy. Eur J Pain 2013.
- 333 16. Harel EV, Rabany L, Deutsch L, Bloch Y, Zangen A, Levkovitz Y. H-coil repetitive
334 transcranial magnetic stimulation for treatment resistant major depressive disorder: An 18-
335 week continuation safety and feasibility study. World J Biol Psychiatry 2012.

- 336 17. Harel EV, Zangen A, Roth Y, Reti I, Braw Y, Levkovitz Y. H-coil repetitive
337 transcranial magnetic stimulation for the treatment of bipolar depression: an add-on, safety
338 and feasibility study. *World J Biol Psychiatry* 2011;12(2):119-26.
- 339 18. Rossi S, Hallett M, Rossini PM, Pascual-Leone A. Safety, ethical considerations, and
340 application guidelines for the use of transcranial magnetic stimulation in clinical practice and
341 research. *Clinical neurophysiology* 2009;120(12):2008-39.
- 342 19. Fugl-Meyer AR, Jaasko L, Leyman I, Olsson S, Steglind S. The post-stroke
343 hemiplegic patient. 1. a method for evaluation of physical performance. *Scand J Rehabil Med*
344 1975;7(1):13-31.
- 345 20. ATS statement: guidelines for the six-minute walk test. *Am J Respir Crit Care Med*
346 2002;166(1):111-7.
- 347 21. Kakuda W, Abo M, Watanabe S, Momosaki R, Hashimoto G, Nakayama Y et al.
348 High-frequency rTMS applied over bilateral leg motor areas combined with mobility training
349 for gait disturbance after stroke: A preliminary study. *Brain Inj* 2013;27(9):1080-6.
- 350 22. Ameli M, Grefkes C, Kemper F, Riegg FP, Rehme AK, Karbe H et al. Differential
351 effects of high-frequency repetitive transcranial magnetic stimulation over ipsilesional
352 primary motor cortex in cortical and subcortical middle cerebral artery stroke. *Annals of*
353 *neurology* 2009;66(3):298-309.
- 354 23. Pascual-Leone A, Valls-Sole J, Wassermann EM, Hallett M. Responses to rapid-rate
355 transcranial magnetic stimulation of the human motor cortex. *Brain* 1994;117 (Pt 4):847-58.
- 356 24. Chen R, Classen J, Gerloff C, Celnik P, Wassermann EM, Hallett M et al. Depression
357 of motor cortex excitability by low-frequency transcranial magnetic stimulation. *Neurology*
358 1997;48(5):1398-403.

- 359 25. Yang YR, Wang RY, Lin KH, Chu MY, Chan RC. Task-oriented progressive
360 resistance strength training improves muscle strength and functional performance in
361 individuals with stroke. *Clin Rehabil* 2006;20(10):860-70.
- 362 26. Chieffo R, Inuggi A, Straffi L, Coppi E, Gonzalez-Rosa J, Spagnolo F et al. Mapping
363 early changes of cortical motor output after subcortical stroke: A transcranial magnetic
364 stimulation study. *Brain Stimul* 2012.
- 365 27. Netz J, Lammers T, Homberg V. Reorganization of motor output in the non-affected
366 hemisphere after stroke. *Brain* 1997;120 (Pt 9):1579-86.
- 367 28. Lotze M, Markert J, Sauseng P, Hoppe J, Plewnia C, Gerloff C. The role of multiple
368 contralateral motor areas for complex hand movements after internal capsular lesion. *J
369 Neurosci* 2006;26(22):6096-102.
- 370 29. Leocani L, Cohen LG, Wassermann EM, Ikoma K, Hallett M. Human corticospinal
371 excitability evaluated with transcranial magnetic stimulation during different reaction time
372 paradigms. *Brain* 2000;123 (Pt 6):1161-73.
- 373 30. Giovannelli F, Borgheresi A, Balestrieri F, Zaccara G, Viggiano MP, Cincotta M et al.
374 Modulation of interhemispheric inhibition by volitional motor activity: an ipsilateral silent
375 period study. *J Physiol* 2009;587(Pt 22):5393-410.
- 376 31. Kapreli E, Athanasopoulos S, Papathanasiou M, Van Hecke P, Strimpakos N,
377 Gouliamos A et al. Lateralization of brain activity during lower limb joints movement. An
378 fMRI study. *Neuroimage* 2006;32(4):1709-21.
- 379 32. Goodwill AM, Pearce AJ, Kidgell DJ. Corticomotor plasticity following unilateral
380 strength training. *Muscle Nerve* 2012;46(3):384-93.
- 381
- 382
- 383

384 **Legends**

385 **Figure 1:** Study design: double-blind placebo-controlled crossover study

386 For both real and sham treatment, 11 rTMS sessions (grey vertical bars) were performed
387 within a 3-week period (5 in the first week and 3 in the second and third weeks), separated by
388 a 4-week wash-out. W: week; T: time of clinical evaluations.

389 **Figure 2:** lower limb FM (Fugl-Meyer) scores grouped according to treatment sequence.

390 Black circles: real-sham sequence (4 subjects) and grey squares: sham-real sequence (5
391 subjects). Continuous lines: rTMS period; dashed lines: wash-out period. In both groups,
392 after real stimulation performance grows even after the end of treatment, while placebo effect
393 fades away.

394 **Figure 3:** (A) lower limb FM (Fugl-Meyer) score: real vs sham comparison (9 vs 9 patients)
395 revealed a significant improvement at the end of treatment ($p=0.01$) as well as at follow-up (p
396 $=0.006$). Amelioration was greater after 4 weeks from the end of real treatment as confirmed
397 by a significant difference in baseline percent change at the end of treatment *vs* follow-up ($p=$
398 0.04).

Table 1 Demographic data, clinical features and treatment sequence of each patient are reported.

Patient	age	lesion	onset (months)	NIHSS	BI	mRS	Sequence
1	50	right capsulo-lenticular ischemia	20	3	90	2	real-sham
2	74	right internal capsular ischemia	21	2	100	1	real-sham
3	65	left capsulo-lenticular hemorrhagia	8	5	100	2	sham-real
4	49	right capsulo-lenticular hemorrhagia	21	5	100	2	real-sham
5	65	right capsular hemorrhagia	10	4	85	2	sham-real
6*	71	right capsular hemorrhagia	30	3	60	3	real-sham
7	74	left capsular ischemia	24	4	95	2	sham-real
8	69	left capsulo-lenticular hemorrhagia	30	6	85	2	real-sham
9	50	left capsulo-lenticular ischemia	21	3	100	1	sham-real
10	55	right capsular ischemia	25	2	100	1	sham-real

* = drop out; M= male; F= female; NIHSS= National Institutes of Health Stroke Scale; BI= Barthel Index; mRS= modified Rankin Scale

Table 2 Performance scores grouped according to treatment type (n=9).

	FM-LL						10 MT						6 MWT					
	baseline	post	FU	Post	FU	baseline	post	FU	Post	FU	baseline	post	FU	Post	FU	baseline	post	
				vs baseline	vs baseline				vs baseline	vs baseline				vs baseline	vs baseline	vs baseline	vs baseline	
Real rTMS	24,7±1,4	26,8±1,5	27,7±1,5	p=0.009	p=0.001	9,4±1,1	8,5±0,9	8,7±0,9	p=0.04	p=0.07	320,6±29,7	338,9±24,9	345,1±30,9	ns	ns			
Sham rTMS	26,2±1,4	26,7±1,4	25,9±1,1	ns	ns	9,2±1,0	9,0±1,1	8,8±0,9	ns	ns	307,4±34,9	325,7±25,2	309,4±27,5	ns	ns			

Values are expressed as mean ± squared error.

FU= follow up, ns= not significant.

Figure 1

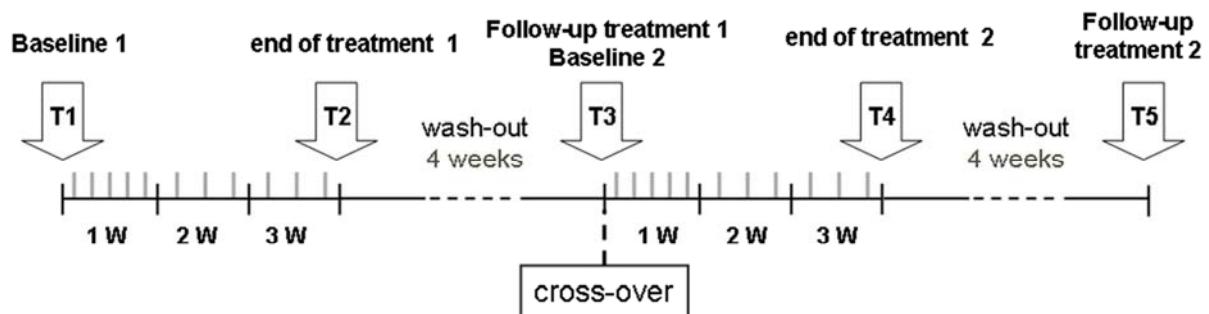


Figure 2

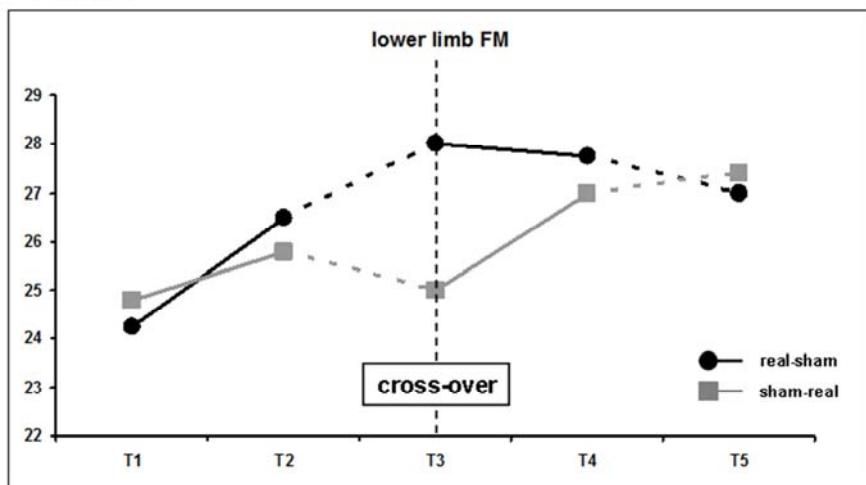


Figure 3

